

The Annual Meeting of the Clinical Nutrition and Metabolism Group of the Nutrition Society with the British Association for Parenteral and Enteral Nutrition, in conjunction with the 24th Congress of the European Society for Parenteral and Enteral Nutrition, was held at the Scottish Exhibition and Conference Centre, Glasgow on 4 September 2002

## Keynote Lecture

# Tissue engineering of the gastrointestinal tract for surgical replacement: a nutrition tool of the future?

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Optimal nutrition depends on the multiple complex functions performed by the gastrointestinal tract, which range from basic functions such as storage, conduit and mechanical processing to more finely regulated capabilities such as vectorial transport, immune defence and cell signalling. Surgical strategies to supply lacking gastrointestinal tract tissues have relied on either replacement by proxy (surgical substitution) or the introduction of prostheses. Tissue engineering seeks to replace missing tissues with engineered tissues that more accurately reproduce the native physiological and anatomical milieu. It is now possible to engineer several areas of the gastrointestinal tract with high fidelity, and to employ tissue-engineered bowel in replacement in animal models. These replacement models have reflected excellent anatomical and physiological recapitulation of native bowel by the tissue-engineered constructs *in vivo*.

### Tissue engineering: Gastrointestinal tract replacement: Animal models

#### Tissue engineering as an evolving field

Optimal nutrition depends on the multiple complex functions served by the gastrointestinal tract, which range from basic functions such as storage, conduit, and mechanical processing to more finely regulated capabilities such as vectorial transport, immune defence, and cell signalling. Surgical strategies to supply lacking gastrointestinal tract tissues have either relied on replacement by proxy (surgical substitution) or the introduction of prostheses. Tissue engineering seeks to replace missing tissues with engineered tissues that more accurately reproduce the native physiological and anatomical milieu. It is now possible to engineer several areas of the gastrointestinal tract with high fidelity, and to employ tissue-engineered bowel in replacement in animal models.

Replacing the physiological purpose and anatomical location of absent gastrointestinal tract tissue, whether due to congenital deficiency or surgical excision, has traditionally been completed in one of two ways. Either a proxy is supplied or a prosthetic non-living substitution is made, such as a

central line and total parenteral nutrition or a colostomy bag serving as a reservoir rather than the living colon.

The limitations of the first approach, native substitution, lie in the dilemma of prioritizing the physiological, psychological and anatomical values of various tissues, and the trade-offs that must be made. In addition, there is a fairly limited supply of donor tissue and it remains inherently different from the tissue it replaces (Grikscheit & Vacanti, 2002). An example is the replacement of the oesophagus with the stomach, colon or jejunal transfer (Belsey, 1965; Jurkiewicz & Paletta, 1989; Dreuw *et al.* 2001; Samuel *et al.* 2001; Gutschow *et al.* 2001). The second approach, artificial substitution, has recognized morbidity: material failure; increased rates of infection; the immune system's destruction of foreign material. Non-living material does not adapt or grow.

A third approach, tissue engineering, has increased in popularity in the last 20 years, with the goal of creating living replacement organs and tissues. By creating the exact tissue that is lacking, self-propagation and self-repair may be gained as well as the possibilities of less physiological

mismatch, rejection and tissue deficit. Progress in the paediatric surgical treatment of short bowel syndrome (Grikscheit & Vacanti, 2002), cranio-facial defects (Lee *et al.* 1997) and valve defects is imminent (Bader *et al.* 1998; O'Brien *et al.* 1999; Shinoka *et al.* 2001). Human application of tissue-engineered skin and large-calibre vessels has already occurred successfully (Shinoka *et al.* 2001). The field of engineered gastrointestinal tract tissue has extended to include all areas of the gastrointestinal tract from the oesophagus to the colon, and even spleen and other solid organs (Grikscheit & Vacanti, 2002).

### Principles of tissue engineering

Organizing complex three-dimensional functional structures from a combination of cells and structural elements relies on numerous spatial and chemical relationships. The multitudinous approaches taken by tissue engineers can be roughly reduced to *in vitro* and *in vivo* designs. There is a requirement for an underlying framework or scaffold for the cells, the proper population of cells and a substitute for the extracellular matrix or extracellular environment. Interactions between cells and extracellular matrix are some of the keys to cell migration, proliferation, differentiation and apoptosis, which are all critical functions for a tissue-engineered construct (Mooney & Langer, 1995).

*In vitro* models have usually relied on the formation of a bioreactor system or cell patterning for monolayer co-culture studies (Folch *et al.* 1999; Zhang *et al.* 1999). Bioreactors are dynamic tissue-culture devices that range from simple mechanical designs to more complex systems with more elements of a living physiological system such as O<sub>2</sub> exchange, defined flow rates and electrical and mechanical stimulation. The engineering of less complex tissues such as cell sheets only requires a simple method to renew the growth medium to the engineered construct and to avoid stasis. Thus, there has been success with models that agitate a growth medium around a construct that has been seeded with cells, such as a spinner flask or rotating vessel (Freed & Vunjak-Novakovic, 1997). More elaborate bioreactors have been designed to furnish stretch to skeletal muscle cultures (Vandenburgh *et al.* 1997), shear to endothelial cells (Wang *et al.* 1996) or compression to chondrocytes (Buckley *et al.* 1998). There is good evidence that engineered tissues grown under physiological conditions including strain and pericellular nutrient availability have improved cell morphology, growth characteristics and metabolic activity (Matas *et al.* 1976; Sutherland *et al.* 1977; Russell, 1985). In studies of chondrocytes subjected to hydrodynamic forces cell proliferation rates are approximately 50% greater and the extracellular matrix is improved (Gupta *et al.* 1991; Balis *et al.* 1999).

*In vivo* studies have focused on animals as a 'physiologically-complete bioreactor', with composite constructs implanted into vascularized spaces such as the omentum, mesentery, interscapular fat pad or *latissimus dorsi* (Vacanti *et al.* 1988). A substitute for the extracellular matrix in the form of a scaffold is implanted after cell loading onto the construct (Lanza *et al.* 2000). The construct can be optimized by modifying the polymer itself through chemical

engineering, microfabrication of topographic cues including the chemical microenvironment or by prevascularization (Uyama *et al.* 1993; Bhatia *et al.* 1998; Kaihara *et al.* 2000a).

A combination of *in vitro* and *in vivo* approaches has solved some simple tissue-engineering problems, and will continue to be equally important for autologous tissue removal, augmentation in the laboratory and eventual *in vivo* replacement.

### Tissue engineering the small intestine

Of the morbid conditions associated with bowel resection, short bowel syndrome may be the most psychologically, economically and qualitatively devastating. Characterized by progressive weight loss, malnutrition, vitamin deficiency and infections associated with the vascular access commonly used to support patients with this syndrome (Wilmore *et al.* 1997), short bowel syndrome usually ensues when less than one-third of the normal small intestine remains, as in cases of massive resection. Surgical attempts to treat this syndrome include bowel transplant (Bueno *et al.* 1999), reversed segments (Diego *et al.* 1982) and recirculating loops (Thompson *et al.* 1984), as well as tapering and lengthening procedures to encourage intestinal mucosa to proliferate (Weber *et al.* 1982; Pokorny & Fowler, 1991). However, there is currently no durable surgical solution.

The ideal tissue-engineered intestinal substitute would be anatomically and microbiologically constructed to model the structure and function of native intestine. In addition, as a self-repairing and self-proliferating tissue replacement, tissue-engineered intestine would grow with the patient and require less maintenance or replacement.

Beginning 12 years ago with the observation that fetal intestine transplanted on polymer scaffolds showed proliferation and intestinal morphogenesis (Vacanti *et al.* 1988), the Boston group has built an expertise in the production of tissue-engineered small intestine. A refinement of these techniques in the past 2 years has led to the generation of better tissue-engineered small intestine and the novel formation of tissue-engineered oesophagus, colon, spleen (Grikscheit *et al.* 2001, 2002, 2003a,b,c) and stomach (Grikscheit & Vacanti, 2003). The generation of a composite tissue resembling small intestine generated from intestinal crypt cells paratopically transplanted as epithelial organoid units was first reported by the Boston group in 1998 (Choi *et al.* 1998). Organoid units are obtained from full-thickness harvests of small intestine. After purification they are loaded onto 10 mm long 2 mm non-woven cylindrical polymers made of polyglycolic acid, coated with polylactic acid and implanted into the omentum. Initial experiments showed production of tissue-engineered small intestine with cyto-differentiation and phenotypic maturation as well as apical staining of brush-border enzymes and basolateral staining for laminin. An Ussing chamber study also indicated similar transepithelial resistance between native intestine and the tissue-engineered construct (Choi *et al.* 1998). On histology, tissue-engineered small intestine has a polarized epithelium with appropriate reconstitution of the other layers of the intestinal wall, and there is substantial vascularization accompanying the growth (Choi *et al.* 1998). Addition of endothelial cells or specific trophic factors does not seem to

be necessary. However, a comparison of small bowel resection, partial hepatectomy and porta-caval shunt in addition to the formation of engineered small intestine showed that small bowel resection and porta-caval shunt both resulted in enhanced formation of engineered intestine by morphometric analysis of the neomucosa and cyst dimensions (Kim *et al.* 1999).

Long-term follow-up after anastomosis of tissue-engineered small intestine to native jejunum after 75 or 80 % small bowel resection in male Lewis rats revealed weight gain, bowel patency and significant ( $P < 0.05$ ) increases in the engineered intestine size (Kaihara *et al.* 2000b; Grikscheit *et al.* 2003a). The engineered small intestine immune cell population is a function of exposure to lumen antigens and time of harvest, but becomes normal after anastomosis (Perez *et al.* 2002). In anastomosed tissue-engineered small intestine mucosa harvested at 20 weeks the density and topographical distribution of immune cell subsets was identical to that of normal jejunum. Epithelial mRNA expression topography of Na<sup>+</sup>-dependent glucose transporters, a bowel Na-glucose co-transporter, is also regenerated in anastomosed engineered small intestine, as is divalent cation transporter 1, an Fe transporter (Tavakkolizadeh *et al.* 2000). The normal distribution patterns of these transporters argue that the engineered intestine shows a considerable resemblance to native jejunum, and underlines the therapeutic potential of this conduit for patients who lack small bowel.

### Tissue engineering the gastrointestinal tract

With refinements of the organoid protocol for engineered small intestine, larger cysts have been created with a larger surface area, and engineered stomach, oesophagus, spleen and large intestine have also been created (Grikscheit *et al.* 2001, 2003b). Tissue-engineered large intestine has been studied in a replacement model *in vivo* with good results both for histology and physiology (Grikscheit *et al.* 2003a,b,c). After removal of the native colon, a small intestine pouch is often created as a reservoir, but inflammation of the pouch, pouchitis, is a common complication. There are also additional post-colectomy morbidities associated with lack of the physiological large intestinal function. The symptoms associated with pouchitis are not trivial, including altered stool frequency, abdominal cramping, fever, and extraintestinal manifestations (Shen *et al.* 2001). Although pouchitis is certainly related in part to host factors, which accounts for an increased incidence of pouchitis in ulcerative colitis as compared with familial adenomatous polyposis, the adaptation of small intestine to large intestinal function must also be important (Moskowitz *et al.* 1986).

A primary advantage of tissue engineering is exact replacement of the function and architecture of the tissue that has been removed rather than replacement by proxy. In rat models substitution of tissue-engineered colon for native large intestine resulted in normal electrolytes, less evidence of dehydration and evidence of bile acid recycling. Animals with a tissue-engineered colon pouch proximal to an ileostomy had a significant ( $P < 0.05$ ) physiological advantage to animals with an end ileostomy alone, including

less weight loss and less relative hyponatraemia. With tissue-engineered colon animals had decreased stool moisture content by 10 %. The presence of a tissue-engineered colon segment additionally raised both serum bile acid content and stool short-chain fatty acids, with higher levels of *n*-butyrate than animals with an end ileostomy. Transit times were more than doubled with tissue-engineered colon (Grikscheit *et al.* 2003a,b,c).

Tissue-engineered stomach and oesophagus have promising histology and initial replacement-model findings (Grikscheit *et al.* 2002; Grikscheit & Vacanti, 2003). Although the stomach and oesophagus have less direct impact on the uptake of nutrients, the use of anatomic and physiological conduit and avoiding the need to be deprived of another portion of the gastrointestinal tract (as in the case of colon substitution for missing oesophagus) have obvious implications for nutritional status.

### The future of tissue engineering for nutrition

With obvious implications for the treatment of many critical nutritional problems, engineered gastrointestinal tract replacements may considerably affect patient care in the coming decade if large animal studies and human results are similar to these initial experimental findings. The ability to deliver engineered gastrointestinal tract tissues with improved surface area, transporter function, immune characteristics and architecture could reverse many devastating nutritional problems. The experimental results reported in the present paper have all relied on omental implantation as a bioreactor system to mature the tissue-engineered portions of the gastrointestinal tract. In cases in which the omentum is no longer present or may not be used, additional engineering solutions may be possible.

With the advent of microelectrical mechanical systems, also used in inertial guidance and navigation (Borenstein *et al.* 1997), Si micromachining has been used to form an improved scaffold for vascular networks. Trench patterns are etched on Si and Pyrex templates with resolution to 10 µm. These patterns recapitulate a vascular network. Endothelial cells and hepatocytes or other parenchymal cells can be cultured on the microelectrical mechanical system template, remaining viable and proliferative, producing albumin (Borenstein *et al.* 1997). The monolayers can then be lifted and formed into a three-dimensional structure. Further studies have confirmed that microfabrication technology can be used to form large sheets of living tissue, and that micromachining lumen surfaces for endothelial cells allows ordered co-culture. The lifted organized layers have been implanted as a permanent graft.

Tissue engineering has evolved rapidly, primarily through synergy between creative engineers, chemists, surgeons, physicists, biologists and scientists in a number of other fields. Progress has occurred through contemporaneous improvement of constructs, cell-cell relationships and surgical approaches. The evolution of bioreactor devices, including microfabricated milieus, has also played an important role. This combination of mechanical engineering with tissue engineering and surgical research holds promise for tissue-engineered solutions to surgical nutritional

problems. The ability to specifically engineer the missing portion of the gastrointestinal tract contributing to nutritional imbalance could improve the precision of some nutritional solutions.

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